### **Non-Fourier Reconstruction Can Prevent Image Dropouts**

<sup>1</sup>National Institute of Mental Health, Bethesda, MD, United States, <sup>2</sup>Dept of Physics, Auburn University, Auburn, Alabama, United States

#### **Introduction:**

Uncompensated through-slice magnetic field gradients cause extensive signal dropouts in full *k*-space rectangular-scan EPI due to the long interval before TE is reached. Techniques to fix this problem include *z*-shimming [1-2] and tailored RF pulses to alter the phase profile through the slice [3]. Herein, we propose another method, which in its simplest form does not need a modified EPI pulse sequence or any time penalty, just a new reconstruction algorithm. This method can also be used in conjunction with other techniques, since it only requires a magnetic field map and new software.

## **The Signal-Magnetization Relationship and non-Fourier Reconstruction:**

The basic problem is that the relationship between the measured signal and the magnetization is no longer precisely the Fourier transform. If we abstract out the x- $k_x$  direction as being acquired too rapidly for dephasing to matter, then the signal at time t after excitation can be modeled as  $S(t) \propto \int_{-\text{FOV}/2}^{\text{FOV}/2} \int_{-h/2}^{h/2} M(y,z) e^{-ik_y(t)y} e^{-i[w(y)t+k_z(t)]z} e^{-R_2^*(y,z)t} dz dy$ , where M(y,z) is the post-RF transverse magnetization density (at t=0), FOV is the field-of-view (in the y-direction), h is the slice thickness,  $k_y(t)$  is the phase-encoding readout,  $k_z(t)$  is the integral of any z-shimming gradients, and w(y) is  $\gamma$  times the spatially-dependent through-slice magnetic field gradient. Idealizing further that the magnetization profile in the zdirection is rectangular, the signal model becomes  $S(t) \propto \int_{-\text{FOV}/2}^{\text{FOV}/2} M(y) e^{-R_2^*(y)t} e^{-ik_y(t)y} \operatorname{sinc}\left[\frac{h}{2}\left(w(y)t + k_z(t)\right)\right] dy$ , where  $\operatorname{sinc}(x) \equiv \sin(x)/x$ . If  $w(y)=0=k_z(t)$ , then this model is the usual Fourier relation between S(t) and M(y). When  $k_z(t)\equiv 0$ , at locations y where  $w(y)h \ge 2\pi/\text{TE}$ , the dephasing is such that  $\operatorname{sinc}\left[\frac{h}{2}w(y)\text{TE}\right] \approx 0$  and virtually no signal is received from such values of y in the vicinity of t=TE; normal Fourier reconstruction results in nearly total signal dropout in these locations. However, if the readout starts soon enough after excitation, the early part of the data will contain some signal from the dropout locations at nonzero values of  $k_v$  (while  $w(y)ht \le 1.5\pi$ , say). The non-Fourier reconstruction model we propose is thus to write the model for the image I(y) as  $S(t) \propto \int_{-\text{FOV}/2}^{\text{FOV}/2} I(y) e^{-ik_y(t)y} \operatorname{sinc}\left[\frac{h}{2}\left(w(y)t + k_z(t)\right)\right] dy$ , and then invert this linear integral equation numerically to solve for I(y); solving this equation requires having a  $B_z$  field map, so that w(y)is known. The discretization is  $S_m = \sum_n e^{-ik_y(t_m)y_n} \operatorname{sinc}\left[\frac{h}{2}(w(y_n)t_m + k_z(t_m))\right] \cdot I_n$ , where *n* is the spatial index and *m* is the temporal index. This is a system of linear equations for the image vector  $[I_n]$  given the data vector  $[S_m]$ , and can be solved using the singular value decomposition (among many possible methods). As mentioned above, the speed of acquisition in the  $k_x$  direction means that normal FFT reconstruction can be used for the  $x - k_x$  inversion; therefore, although the matrix is dense, it can be solved quickly since it will involve (typically) only 64-128 unknown values. Once the subject- and

# **Preliminary Results and Discussion:**

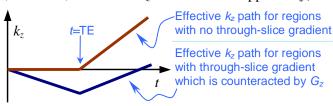
Simulated data were generated that correspond to a realistic EPI acquisition: 27 ms readout window starting at 6 ms after the center of the slice excitation RF; 64 data points in  $k_y$  with a 240 mm FOV; localized 100 Hz through-slice frequency change. The results show that knowing w(y) to within 10% provides an accurate image reconstruction.

orientation-specific gradient field map  $w(x,y) = \gamma \partial B_z(x,y,z)/\partial z\Big|_{z=0}$  is available, the SVD for each slice and each x can be

precomputed, and the overall reconstruction speed for a long imaging run of EPI data will be very fast.

Using a nonzero compensating  $k_z(t)$  for the second half of the acquisition provides a way to gain a second partial acquisition of data from "bad" regions. We keep  $G_z$ =0 until t=TE; for t>TE, a constant  $G_z$  is turned on to oppose w(y).

Simulations show that this type of compensation, coupled with non-Fourier reconstruction, is less sensitive to errors in the estimated w(y) and to noise. Further work is planned to estimate the sensitivity to  $R_2^*$  changes and global field offsets, determine the PSF, choose the  $k_z(t)$  compensation path optimally, &c.



### **References:**

[1] Glover GH, MRM 42: 290-299, 1999. [2] Song AW, MRM 46: 407-411, 2001. [3] Pipe JG, MRM 33: 24-33, 1995.